

Modeling for Quantitative Assessment of Regional Myocardial Blood Flow

Hidehiro Iida, PhD in Physics, PhD in Medical Science

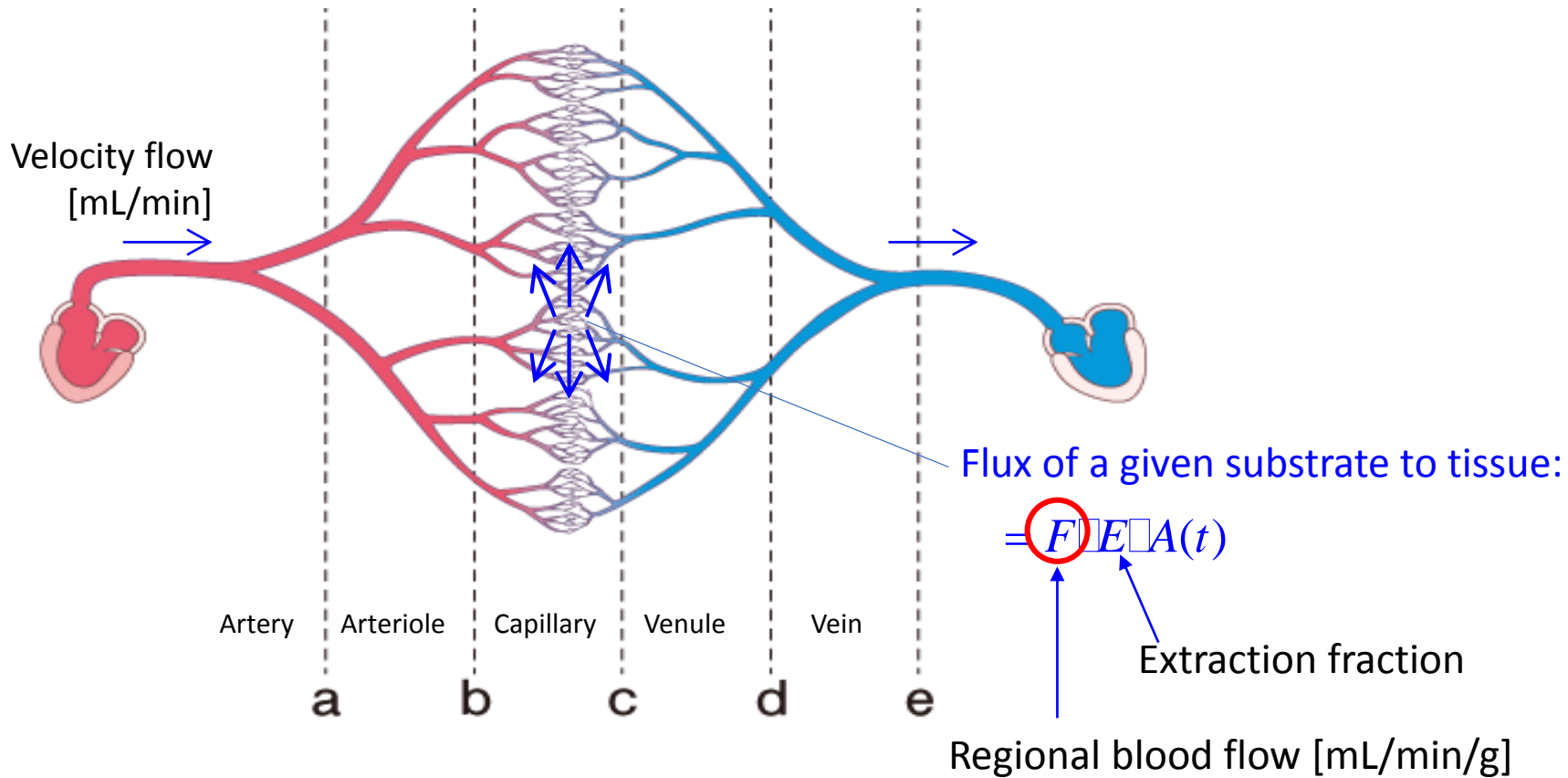
Turku PET Centre, Finland

Modeling, instrumentation, and data analysis in PET, SPECT, and MRI

What is regional myocardial blood flow?

- **Blood flow** (Velocity flow of “blood”)
- **Regional tissue blood flow** (perfusion)
A rate that supplies substrates to regional tissue with a separately defined extraction rate through the capillary membrane

What is regional myocardial blood flow?



Given E of a radio-tracer,
 $F \cdot E$ is practically given as
"regional blood flow"

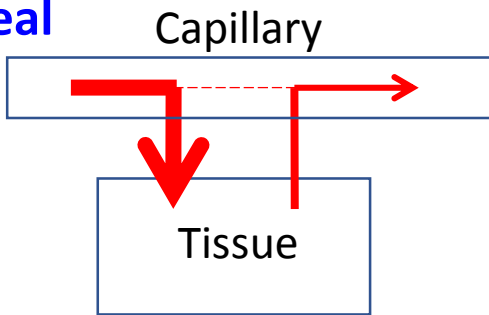
Radiotracers for myocardial perfusion in PET and SPECT

^{15}O-water	2.04 min (PET)	Onsite cyclotron
^{13}N-ammonia	9.96 min (PET)	Onsite cyclotron
^{18}F-flurpiridaz	109 min (PET)	Delivery/cyclotron
^{82}Rb	1.27 min (PET)	Generator
^{62}Cu-PTSM	9.74 min (PET)	Generator
^{201}Tl	72 hour (SPECT)	Delivery
$^{99\text{m}}\text{Tc}$-MIBI ($^{99\text{m}}\text{Tc}$-tetrofosmine)	6.01 hour (SPECT)	Generator/Delivery

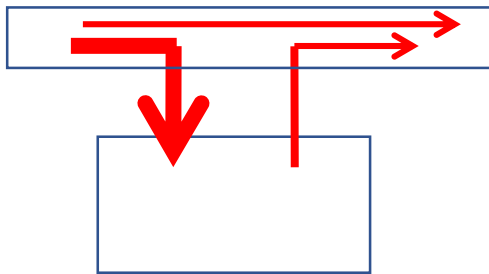
First-pass extraction fraction

$$\frac{dC_i(t)}{dt} = \underbrace{E}_{\text{circled}} \cdot f \cdot Ca(t) - \underbrace{E}_{\text{circled}} \cdot f \cdot C_v(t)$$

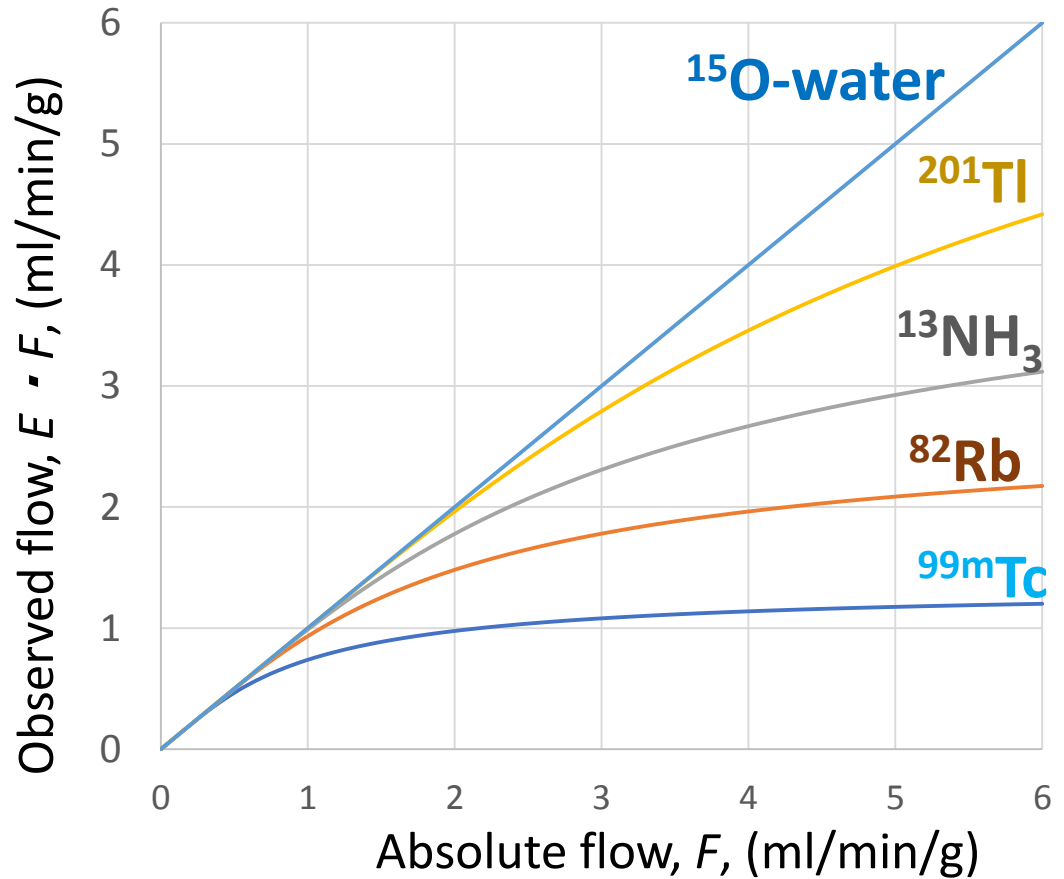
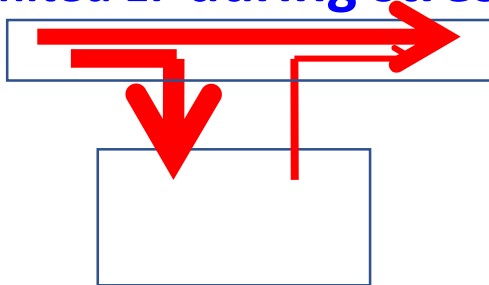
Ideal



Limited EF at rest

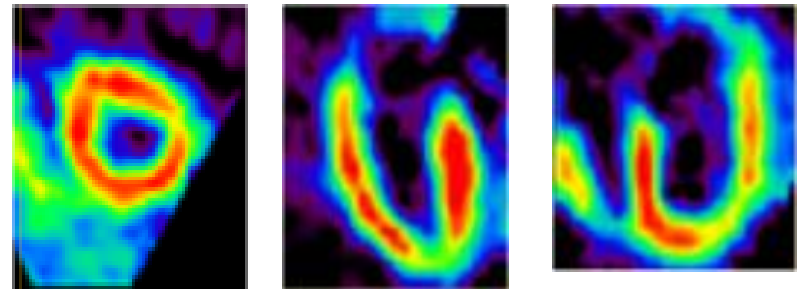


Limited EF during stress



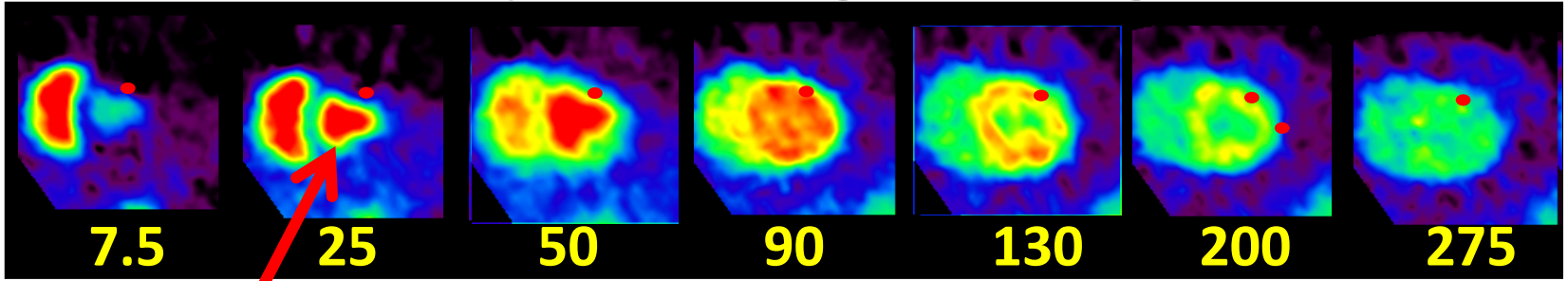
Use of ^{15}O -Water and PET for quantitative assessment of MBF

- ◆ Freely diffusible tracer
- ◆ Allows accurate quantitation of tissue perfusion including PVE correction
- ◆ Short half-life (2min)
- ◆ Allows repeated measurements
- ◆ Additional information of water-perfusible tissue fraction

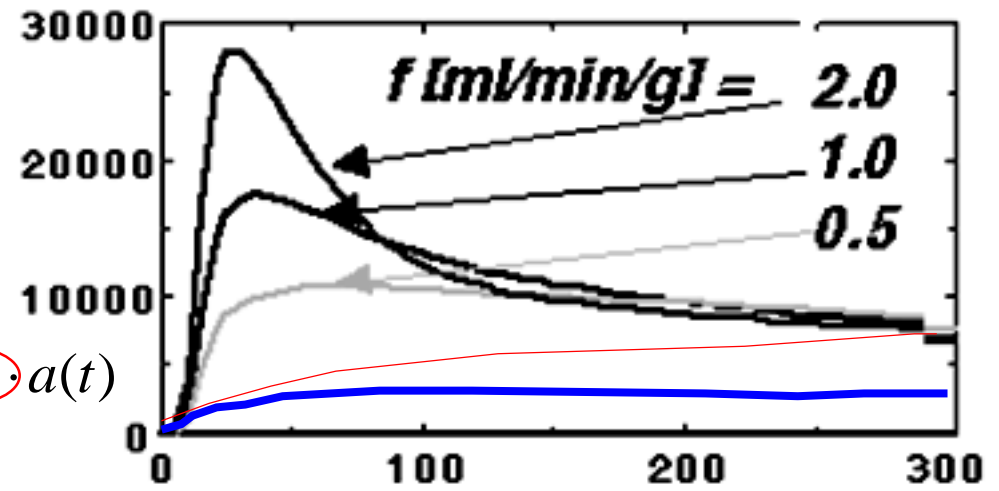
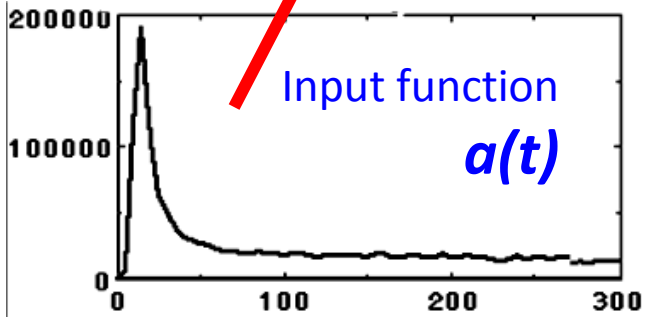


Kinetics of ^{15}O -Water in regional tissue

Sequential Myocardial Images following i.v. ^{15}O -Water



Seconds after I.v. Injection



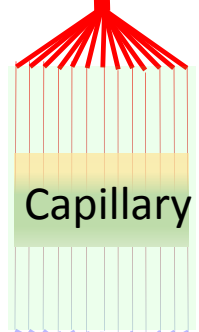
$$R(t) = \text{PTF} \cdot \text{MBF} \cdot a(t) \otimes e^{-\frac{\text{MBF}}{p} \cdot t} + V_a \cdot a(t)$$

↓
MBF, PTF, V_a

Instantaneous equilibrium of water in tissue

Small molecules reaches equilibrium distribution among capillary network

Artery

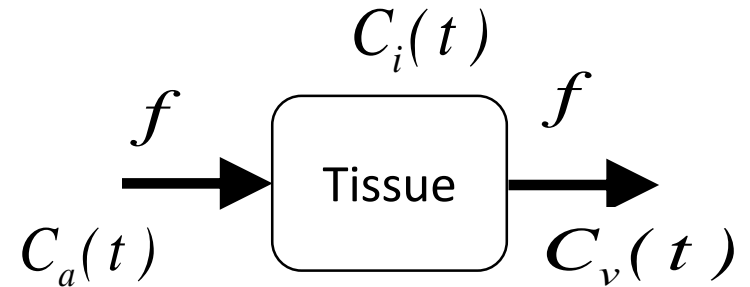
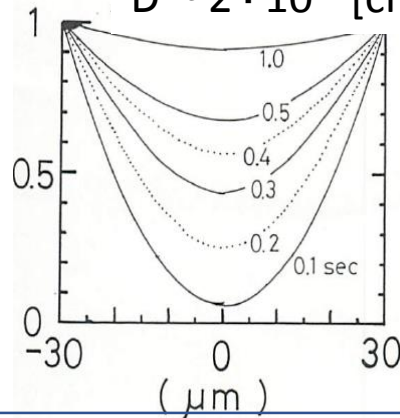


Capillary

Vein

$$\frac{\partial u(t,r)}{\partial t} = D \frac{\partial^2 u(t,r)}{\partial r^2}$$

$$D \sim 2 \cdot 10^{-5} \text{ [cm}^2/\text{s]}$$



$$\frac{dC_i(t)}{dt} = f \cdot C_a(t) - f \cdot C_v(t)$$

$$\frac{dC_i(t)}{dt} = f \cdot C_a(t) - f \cdot \frac{C_i(t)}{p}$$

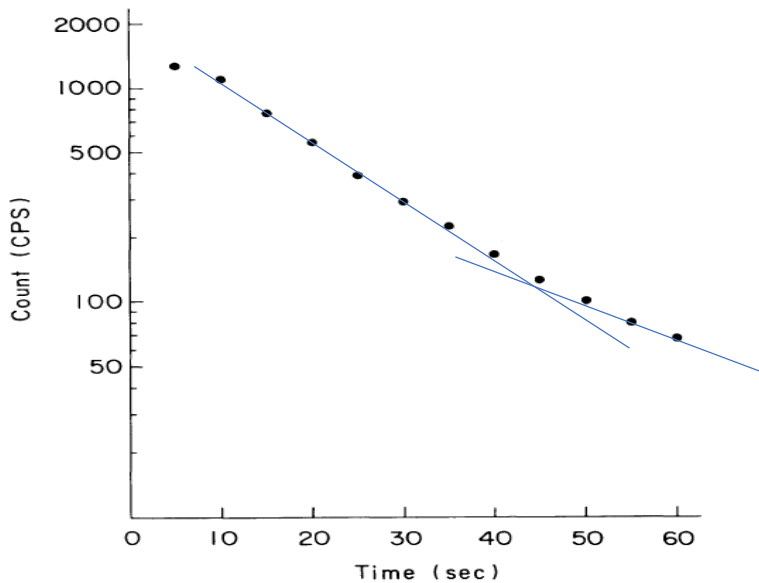
$$\therefore C_v(t) = \frac{C_i(t)}{p}$$

$$C_i(t) = f \cdot C_a(t) \otimes e^{-\frac{f \cdot t}{p}}$$

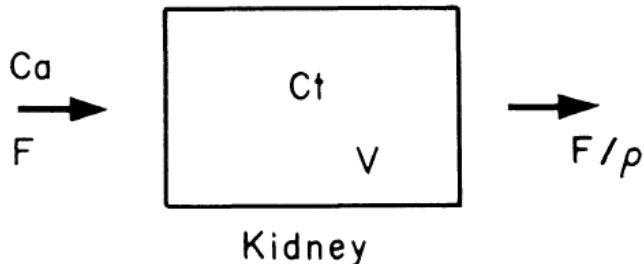
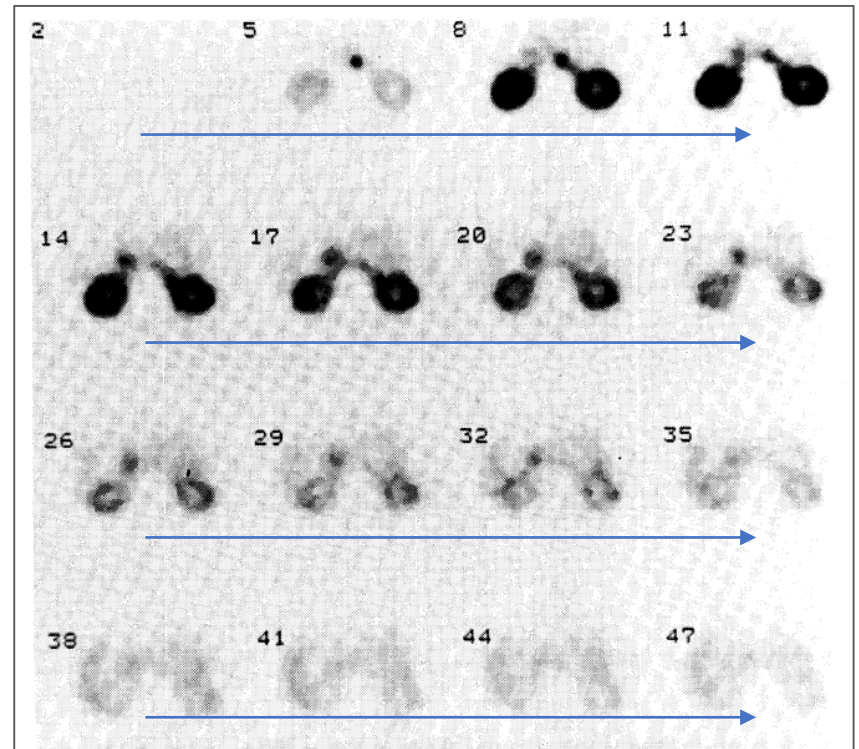
Tissue TAC Input function Regional flow

Kinetic model for regional kidney blood flow using ^{15}O -water and PET

Clearance curve after bolus injection of ^{15}O -water into Kidney artery



Sequential images after bolus injection of ^{15}O -water into Kidney artery



$$\frac{dC_t(t)}{dt} = F \cdot C_a(t) - \frac{F}{\rho} \cdot C_t(t)$$

or $C_t(t) = e^{-(F/\rho)t}$

Partial Volume Effect (PVE) in myocardial PET

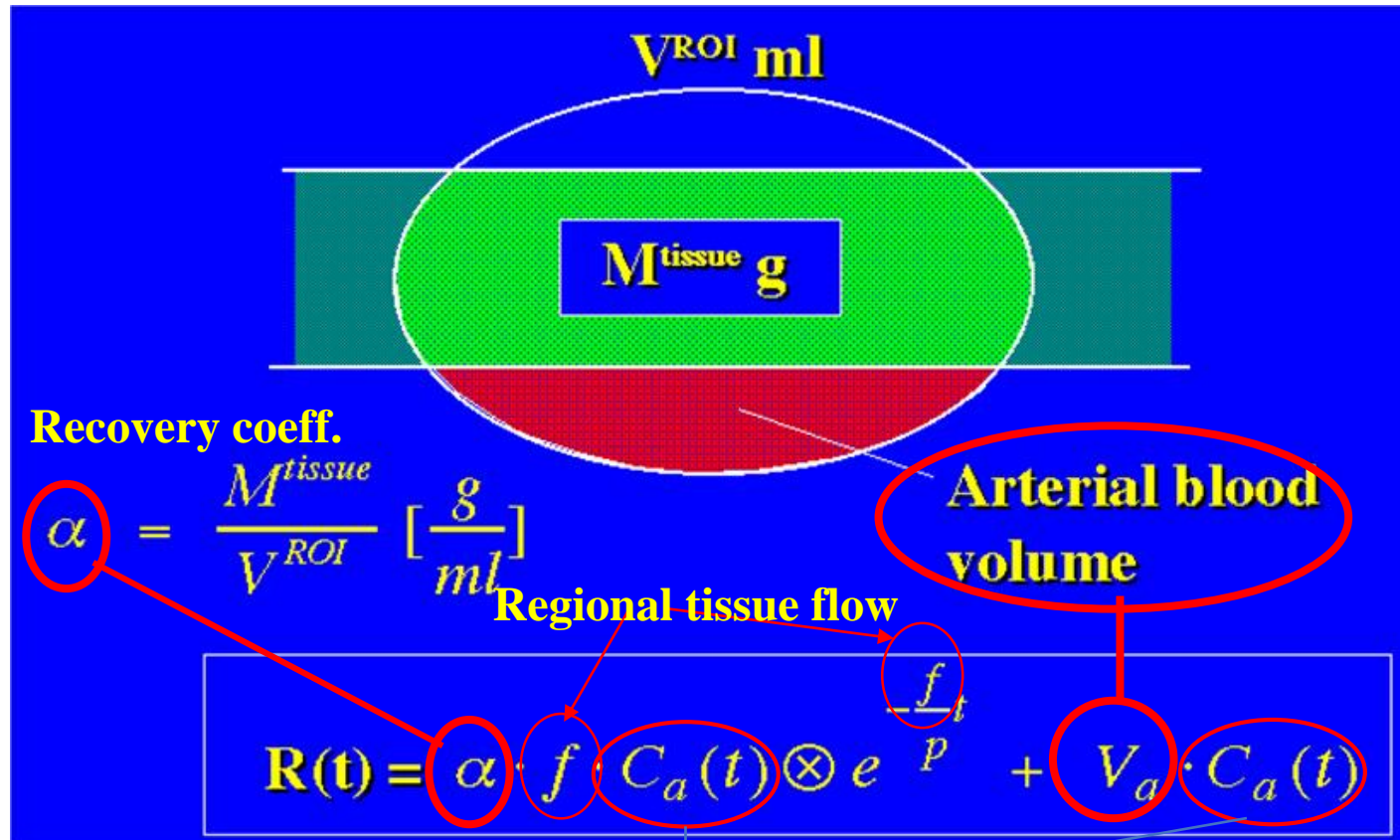


- PET provides radioactivity concentration in Bq per unit volume element [Bq/mL]
- For objects with small structure having the radioactivity concentration of Bq per unit mass [Bq/g-tissue], PET underestimates the radioactivity concentration:

$$PET \left[\frac{Bq}{mL} \right] = \alpha \left[\frac{g}{mL} \right] \cdot Tissue\ Concentration \left[\frac{Bq}{g} \right]$$

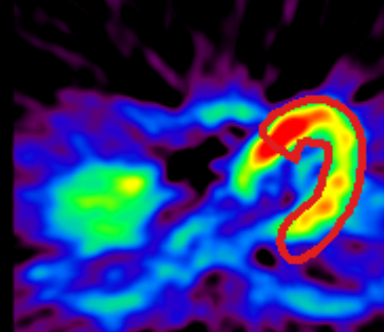
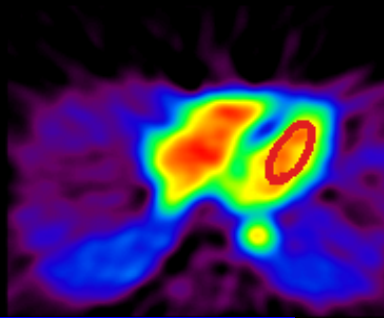
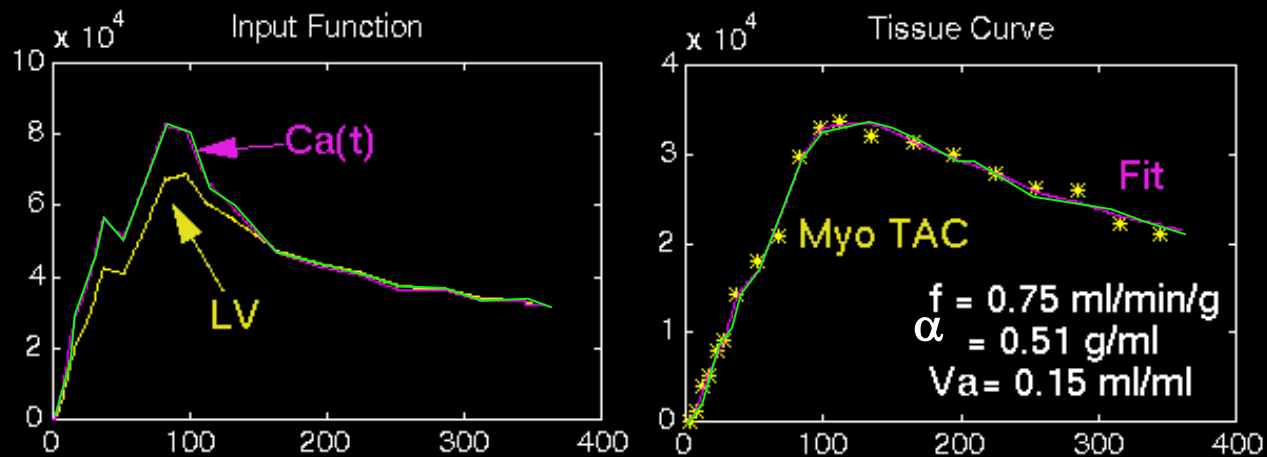
Compartment model for Myocardial ^{15}O -water PET

Unique approach to correct for partial volume effect



Can be estimated from LV chamber TAC on PET images

An example of data analysis for ^{15}O -Water PET for regional myocardial blood flow

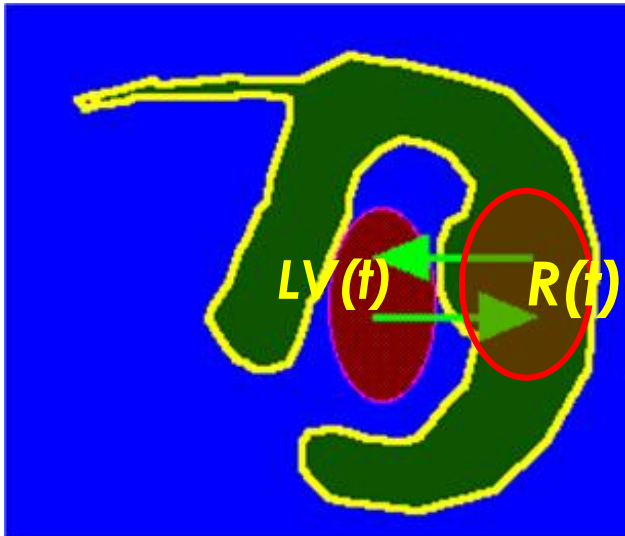


$$\alpha = \frac{M^{\text{tissue}}}{V^{\text{ROI}}} \left[\frac{\text{g}}{\text{ml}} \right]$$

$$R(t) = \alpha \cdot f \cdot C_a(t) \otimes e^{-\lambda t} + V_a \cdot C_a(t)$$

Use of LV TAC and Spillover Correction In Myocardial ^{15}O -water PET

Unique approach to correct for partial volume effect



$$R(t) = \alpha \cdot C_i(t) + V_a \cdot C_a(t)$$
$$LV(t) = \beta \cdot C_a(t) + \gamma \cdot C_i(t)$$
$$= \beta \cdot C_a(t) + (1 - \beta) \cdot C_i(t)$$

$$\because \beta + \gamma = 1$$

$$C_i(t) = \alpha \cdot f \cdot C_a(t) \otimes e^{-(f/p) \cdot t} + V_a \cdot C_a(t)$$

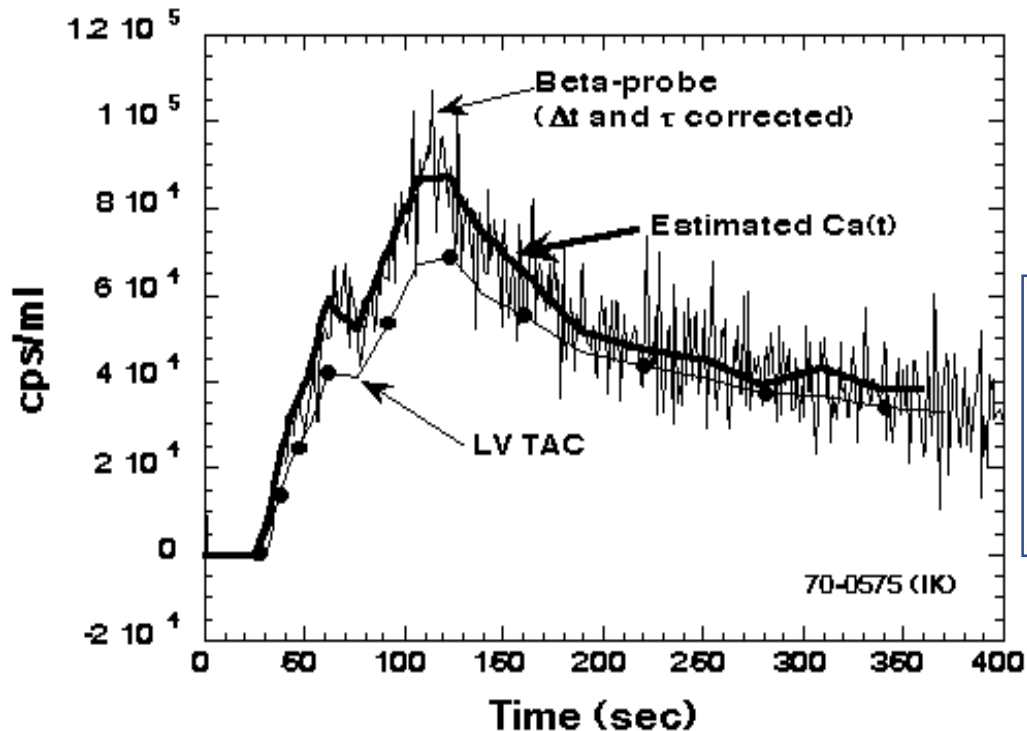
For a given β -value,

fitting f , α and V_a to $R(t)$ and $LV(t)$ enables estimation of $Ca(t)$

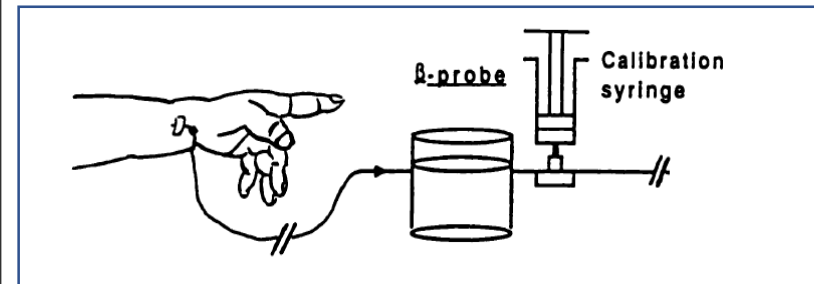
Important that a correct β value is given, and that $\beta + \gamma = 1$ is a good approximation

Validation of ^{15}O -Water PET for quantitation of regional myocardial blood flow

Validation of LV Input Function in ^{15}O -Water PET

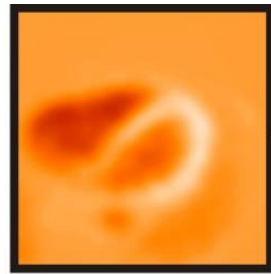


Continuous arterial blood sampling & monitoring radioactivity concentration in the catheter tube



From Iida et al., *J Nucl Med* 1998;39:1789-1798

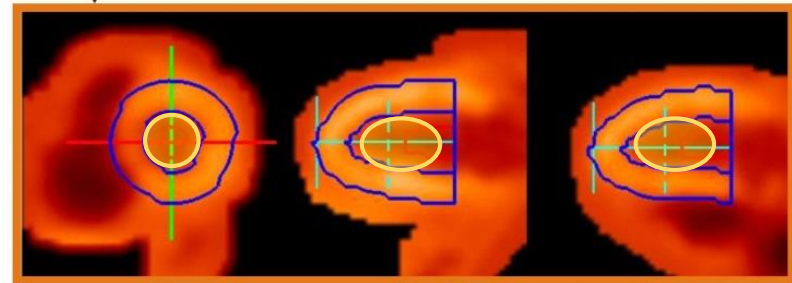
Analysis of dynamic PET Imaging: ^{15}O -water



A difference image of a heart water study



The reoriented image

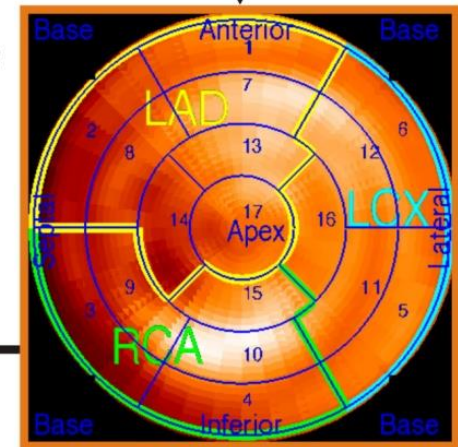


The ROI definition step



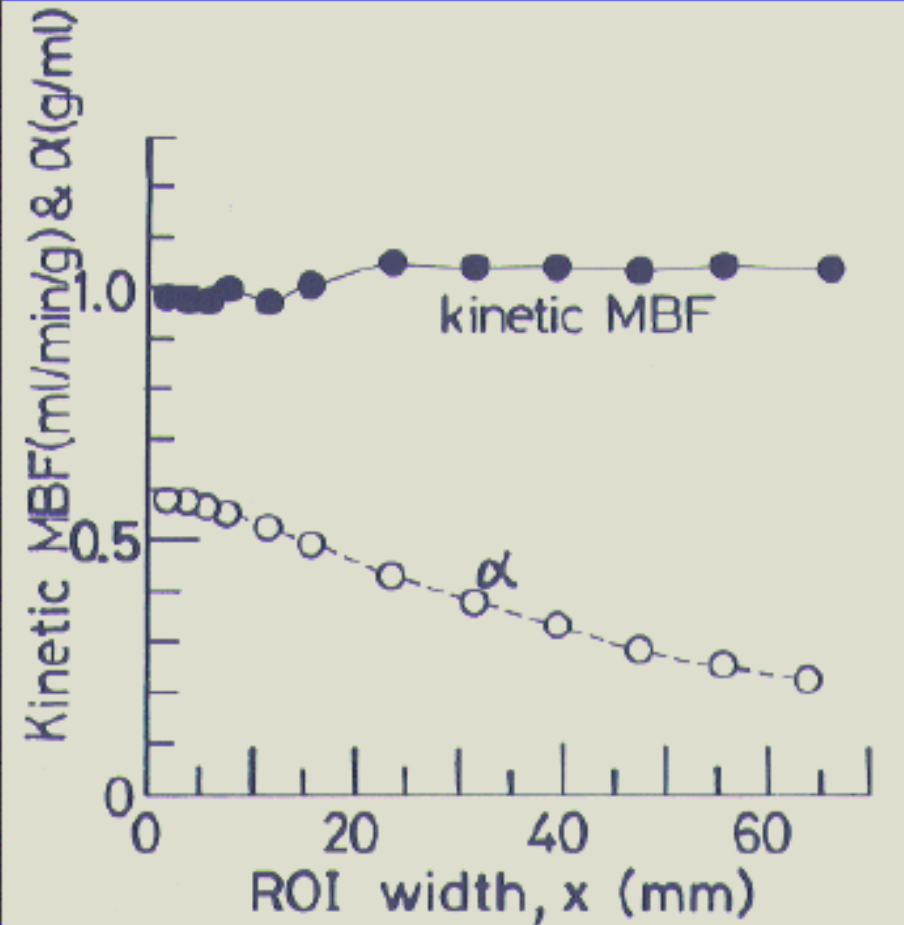
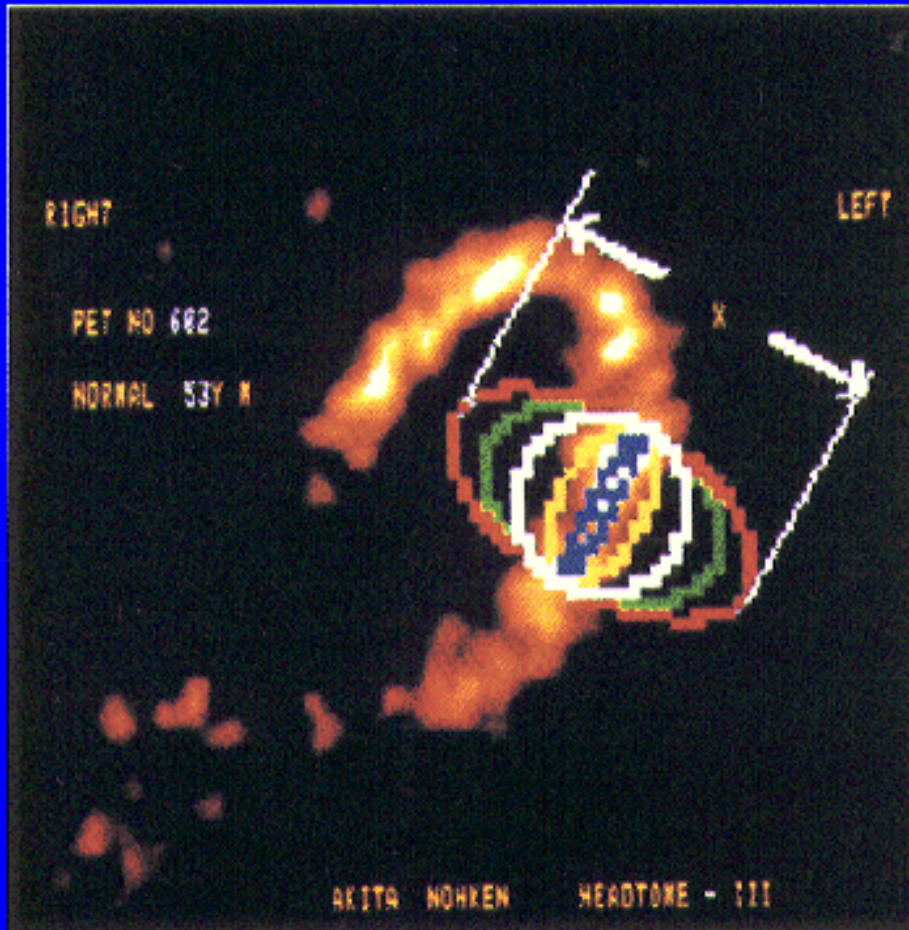
The hybrid PET/CT image

The polar plot



Validation of MBF Quantification by Use of O-15 Water

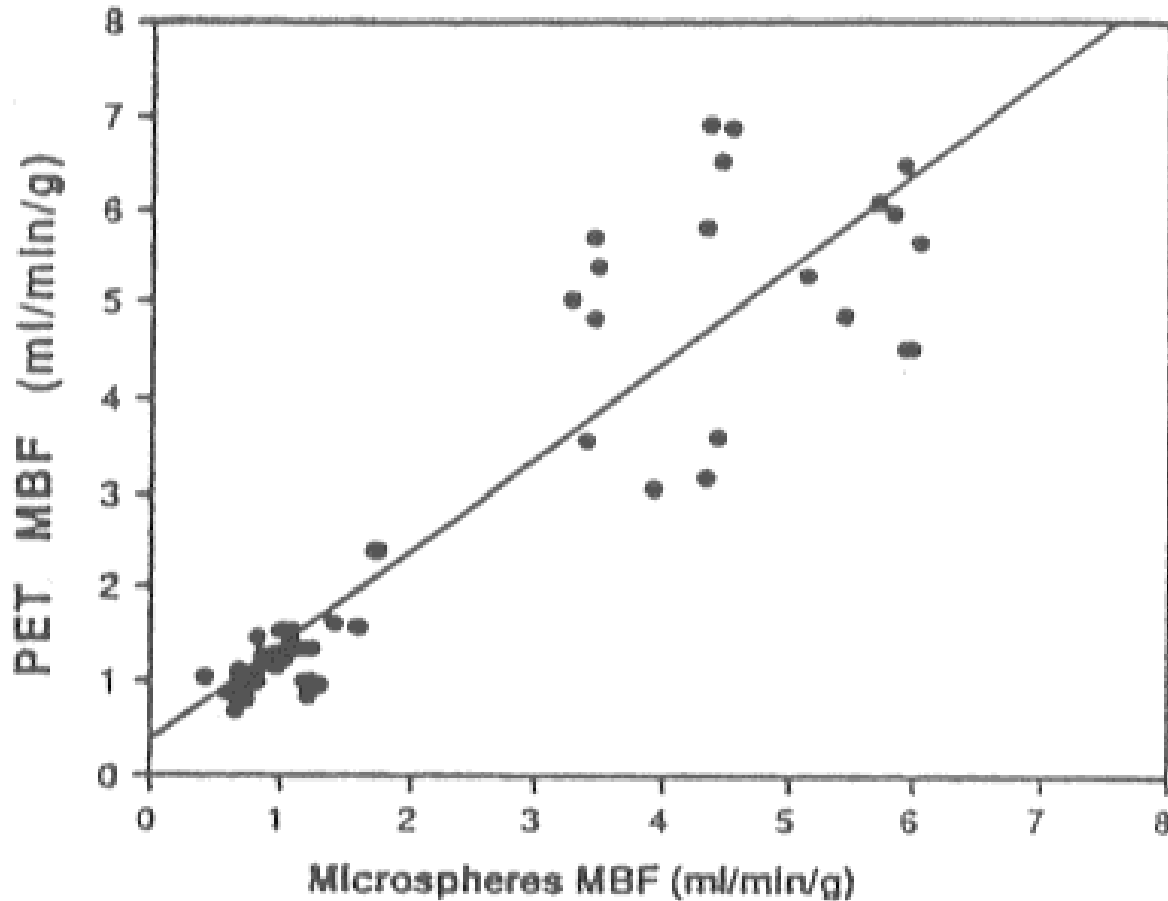
ROI Size Dependency of Estimated MBF



Iida H, Circulation 78:104-115, 1988

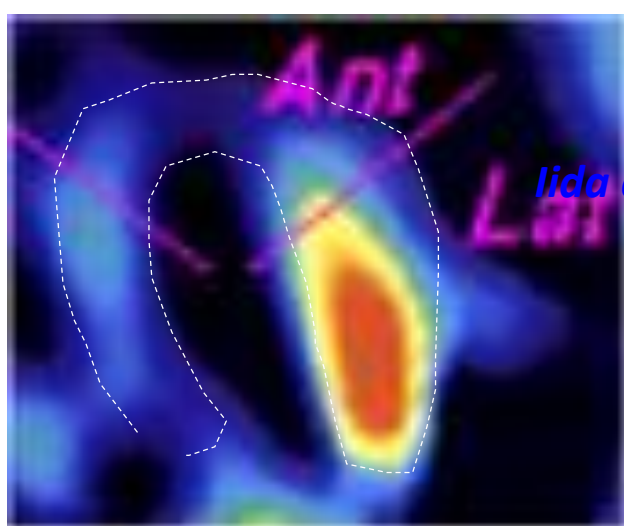
Validation of ^{15}O -Water PET for quantitation of regional myocardial blood flow

PET MBF and Microspheres MBF in Dogs

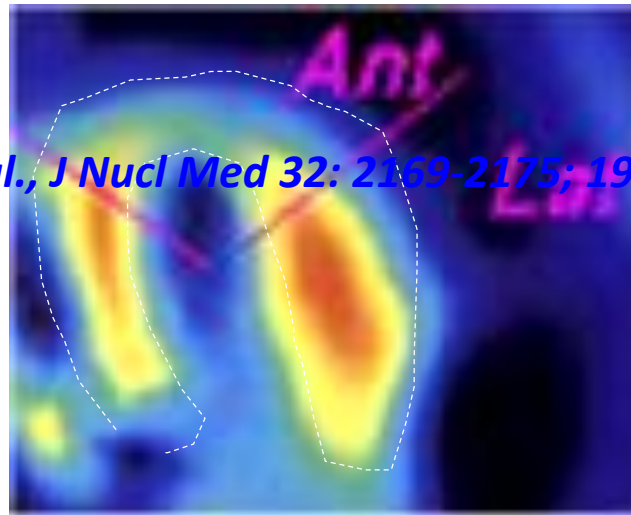


Araujo et al., Circulation 1989

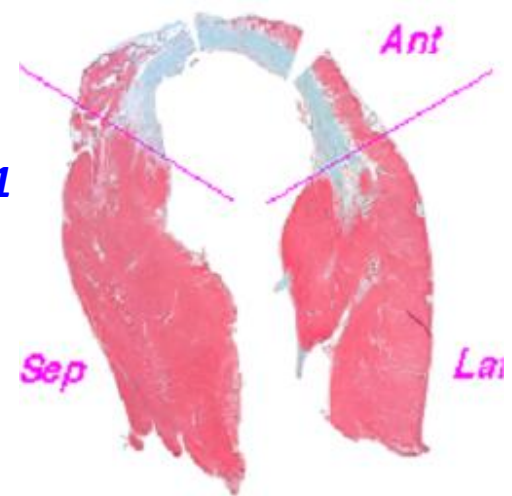
MBF and water-perfusable tissue (PTF) by ^{15}O -water PET in a K9 model of OMI



MBF
(ml/min/mL)



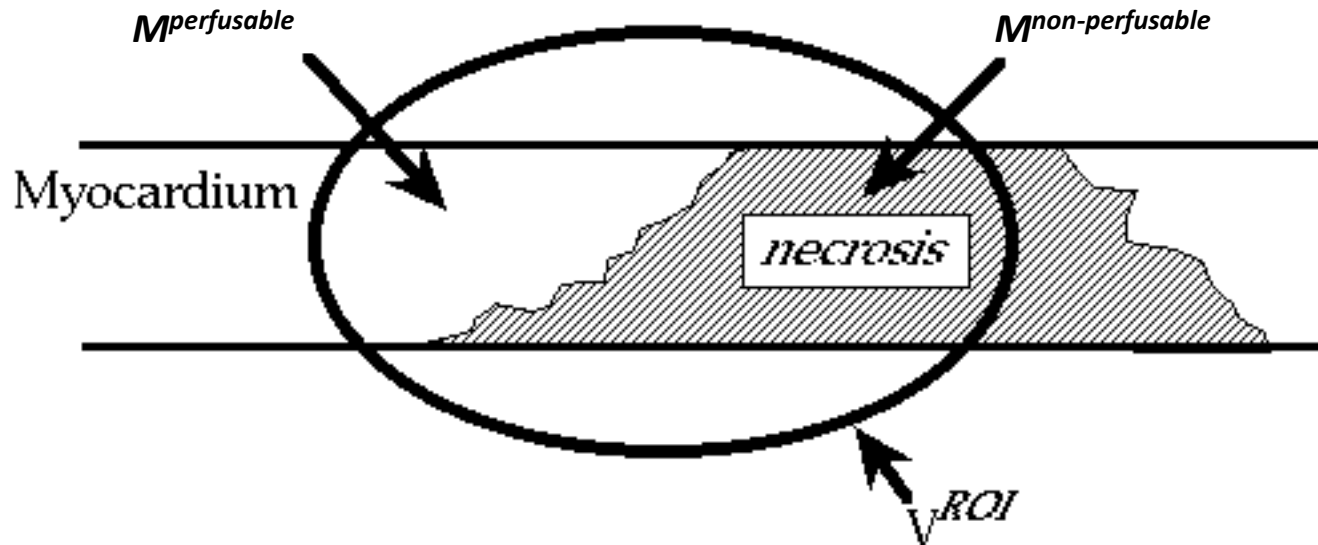
PTF
(g/mL)



EM

Iida et al J Nucl Med. 41:1737-1745., 2000

Water perfusable tissue fraction in the area of myocardial infarction



$$PTF (\alpha) = M^{perfusable} / V^{ROI}$$

$$ATF (Dev) = (M^{perfusable} + M^{non-perfusable}) / V^{ROI}$$

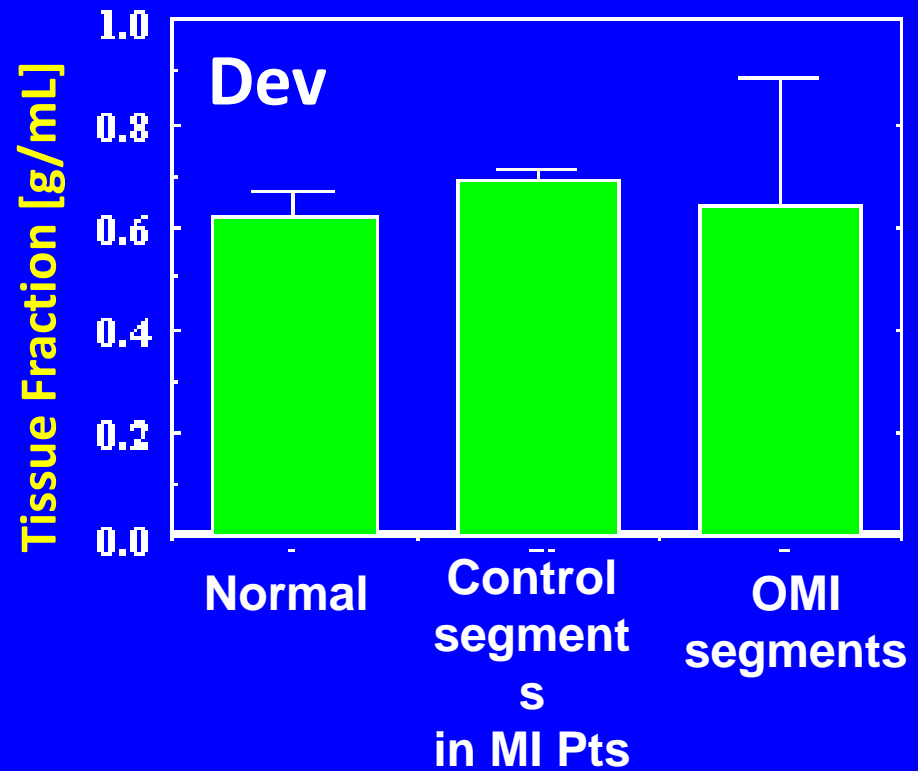
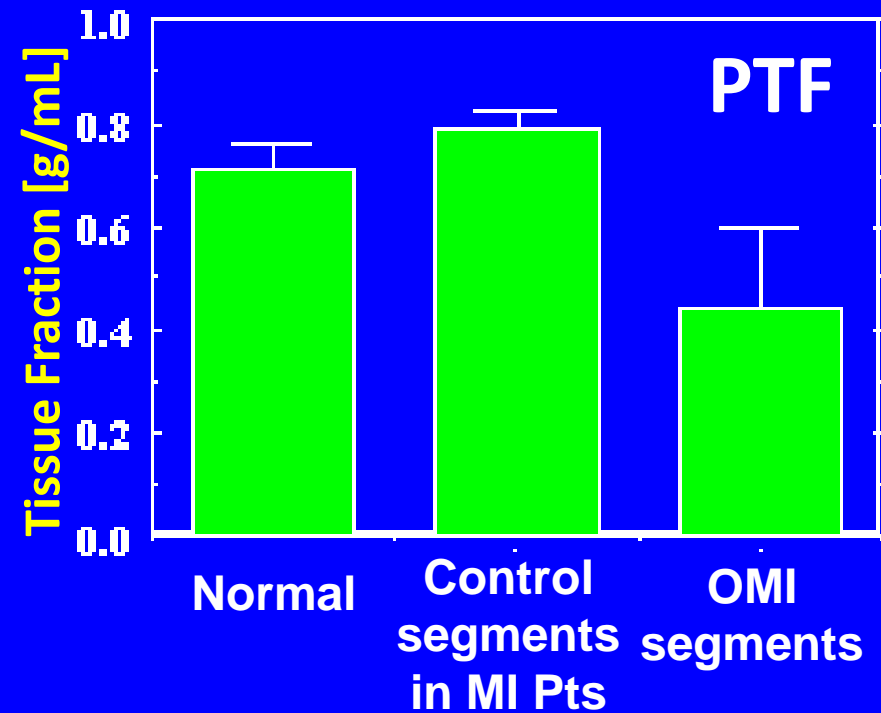
$$PTF \leq Dev$$

$$PTI \equiv PTF/Dev = M^{perfusable} / M^{total}$$

Functional vs Anatomical PVE Correction Factor

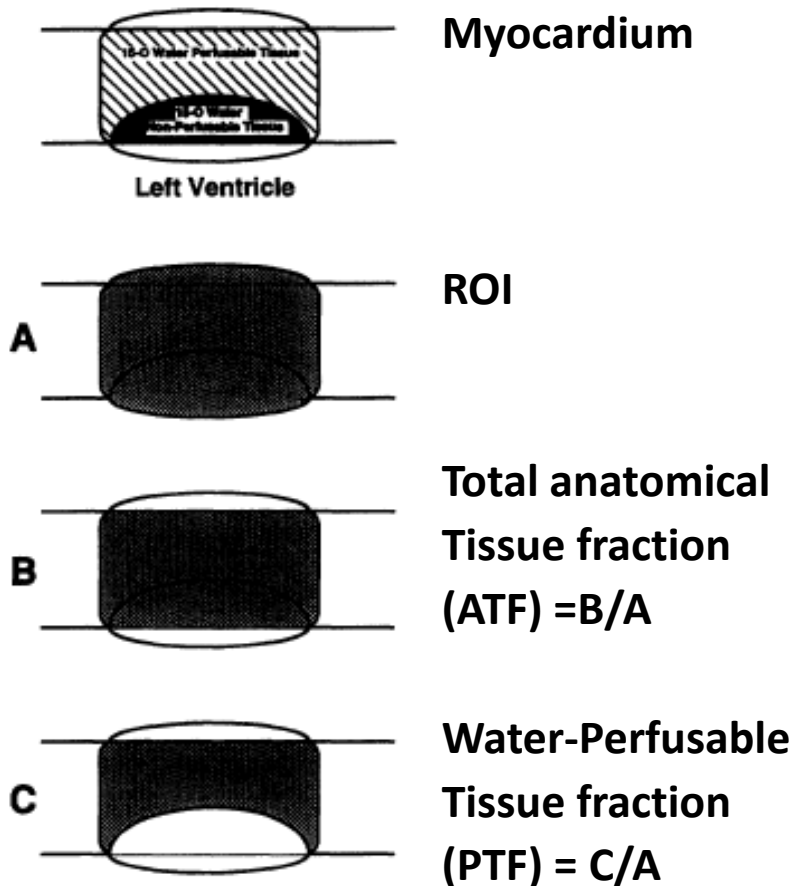
$H_2^{15}O$ -Derived Tissue Fraction

Anatomically-Derived Tissue Fraction

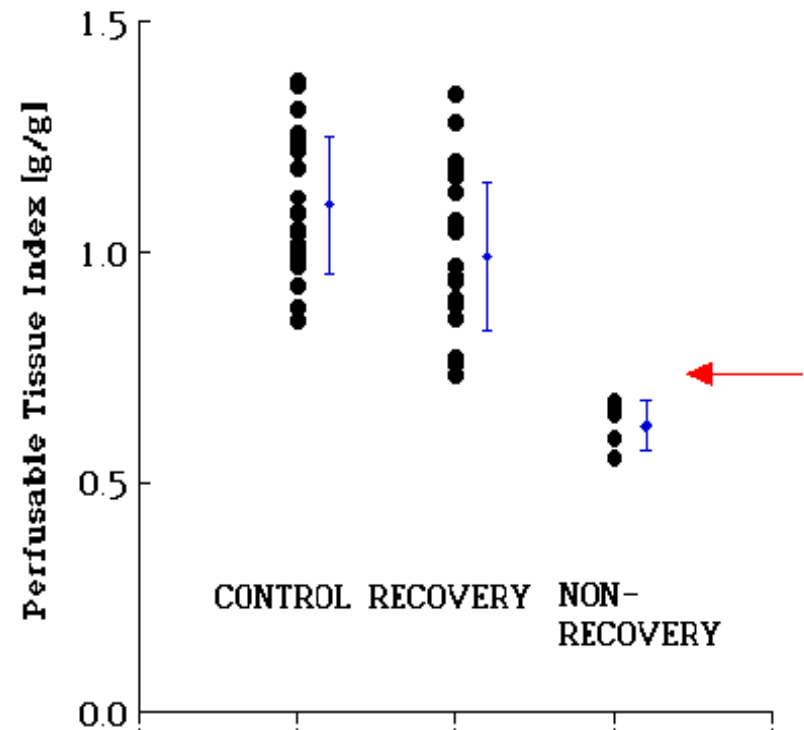


Iida et al., J Nucl Med, 1991

PTI as a Myocardial Viability Marker



PTI values before CABG



Yamamoto et al, Circulation, 1992
De Silva et al, Circulation, 1993

Perfusable Tissue Index as a Potential Marker of Fibrosis in Patients with Idiopathic Dilated Cardiomyopathy

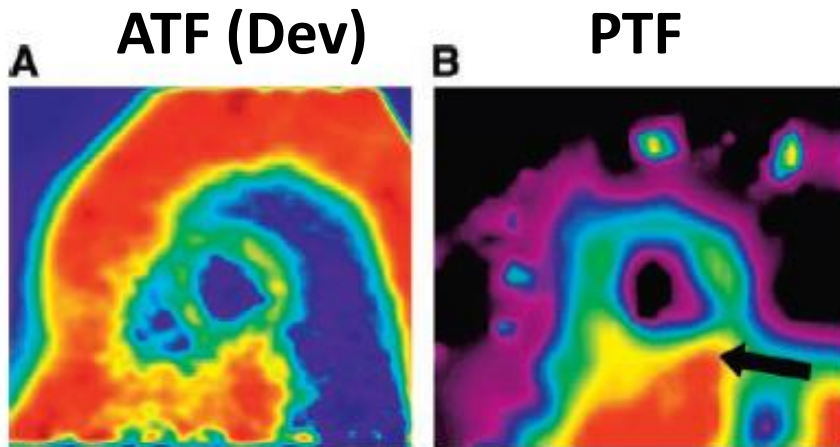


FIGURE 1. Short-axis ATF (A) and PTF (B) images of a healthy volunteer. Arrow in PTF image indicates inferior wall. Spillover effects from adjacent liver tissue are present.

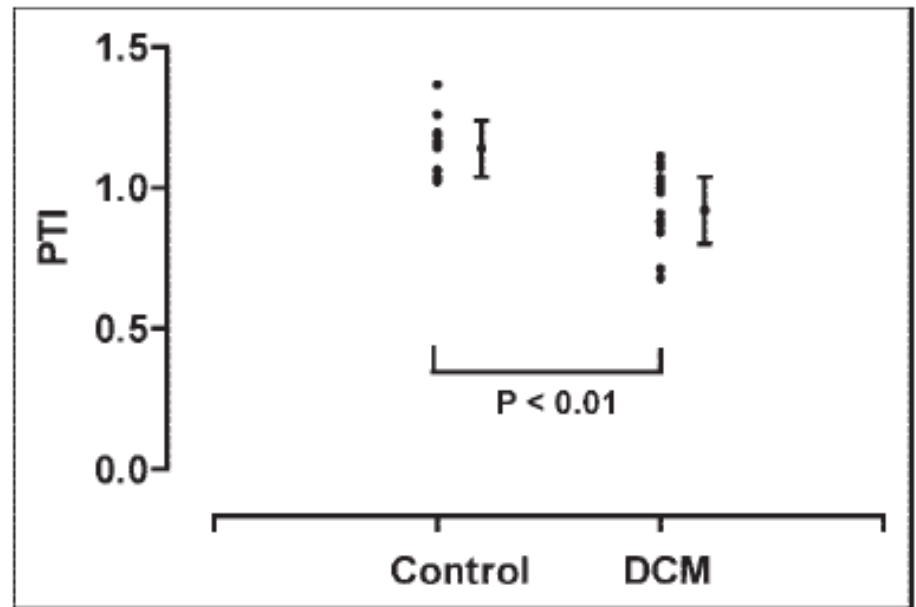
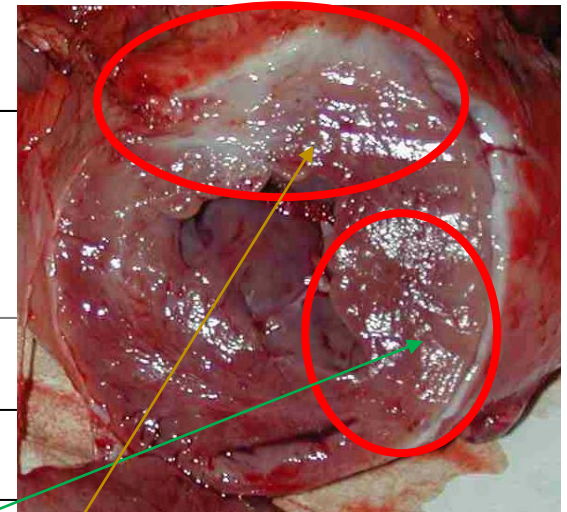
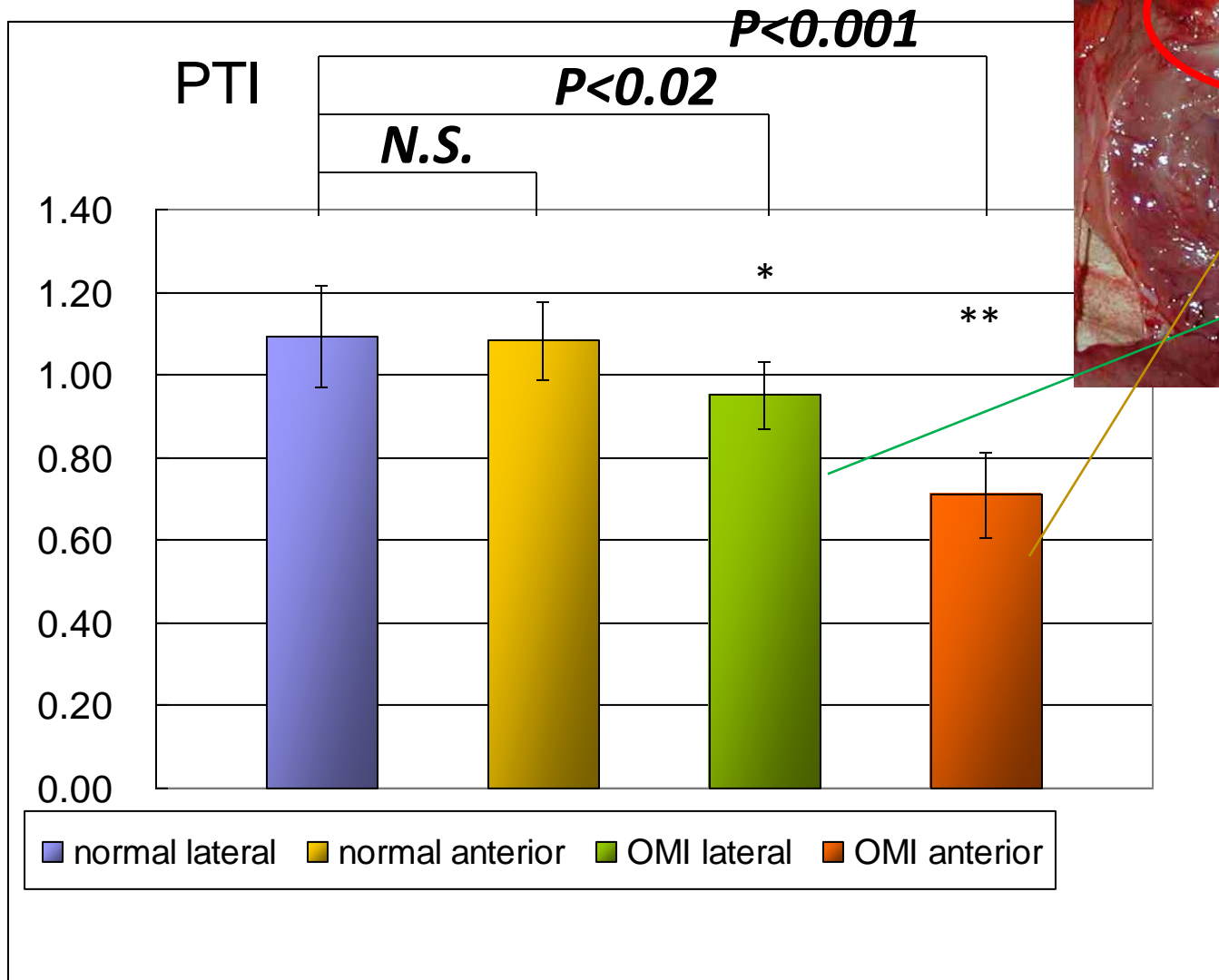


FIGURE 2. PTI for healthy control subjects and DCM patients.

PTI in Pigs with OMI



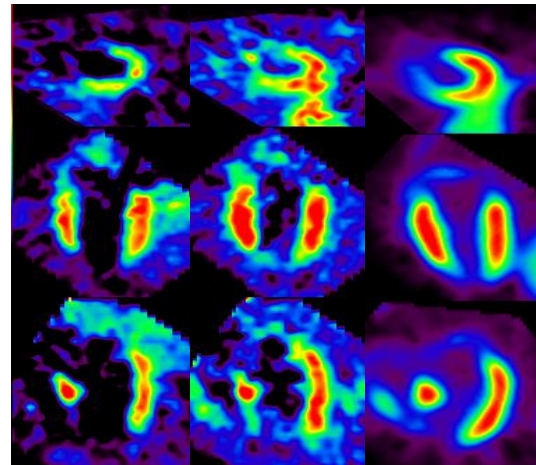
Sham-operated vs myoblast-transplanted myocardium in farm pigs with OMI

Sham operated

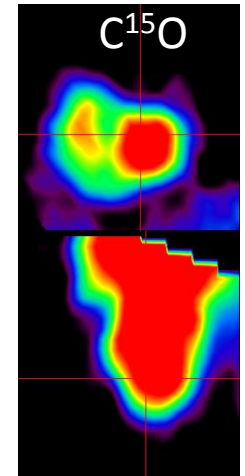


mpigh02_96n

MBF PTF FDG



Gated bloodpool

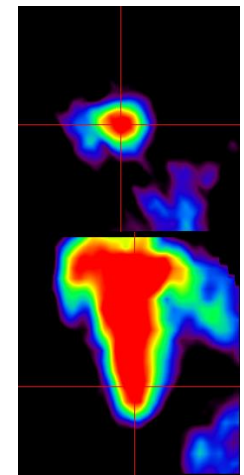
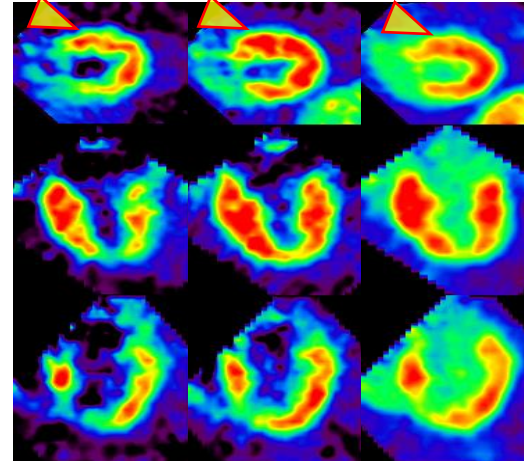


Autologous myoblast transplanted



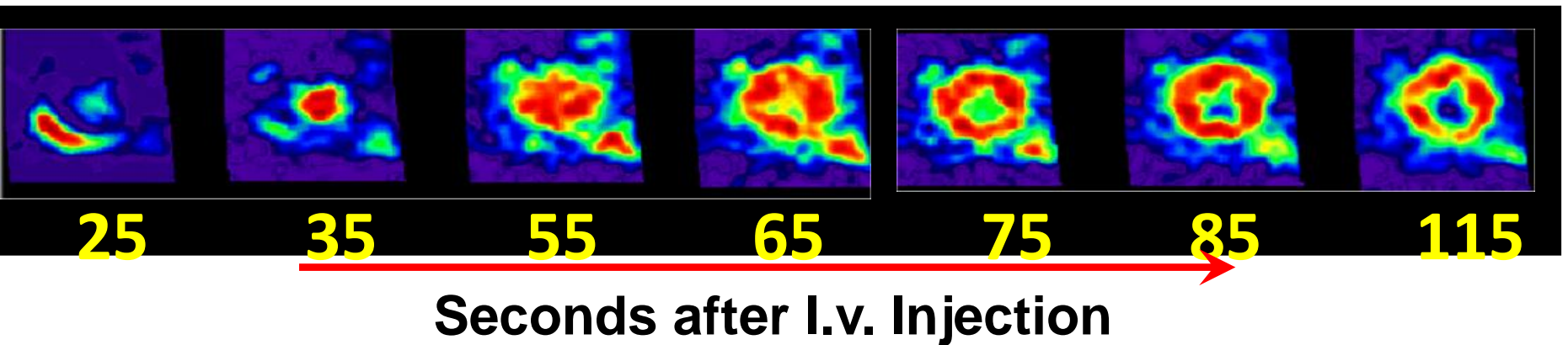
mpigh22_9bp

MBF PTF FDG

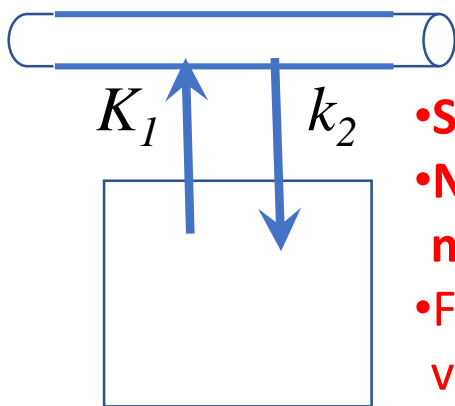


MBF quantitation with $^{13}\text{NH}_3$

metabolism-based accumulation

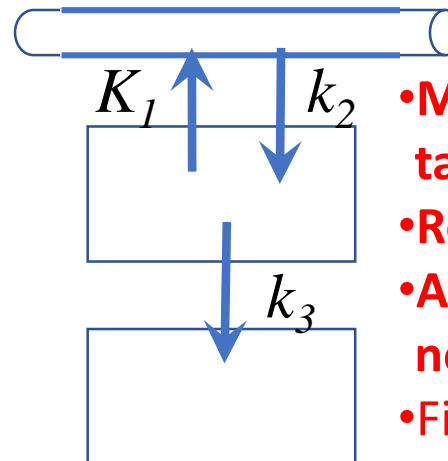


2-tissue compartment model



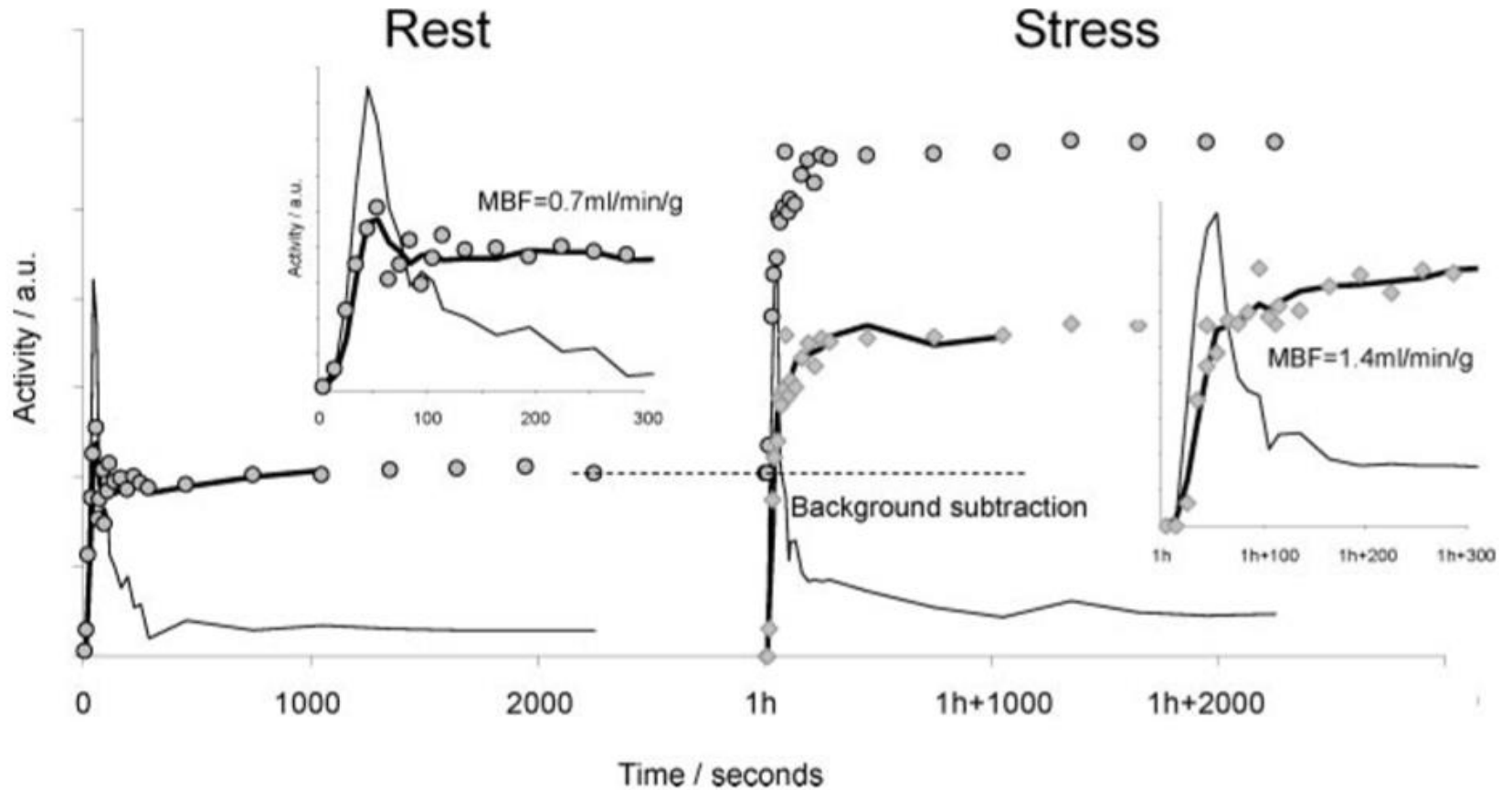
- Short period scan
- Negligible arterial metabolite
- First-pass EF, partial volume effect, etc need to be corrected

3-tissue compartment model



- Metabolic retention taken into account
- Requires longer scan
- Arterial metabolite not-negligible
- First-pass EF, partial volume effect, etc need to be corrected

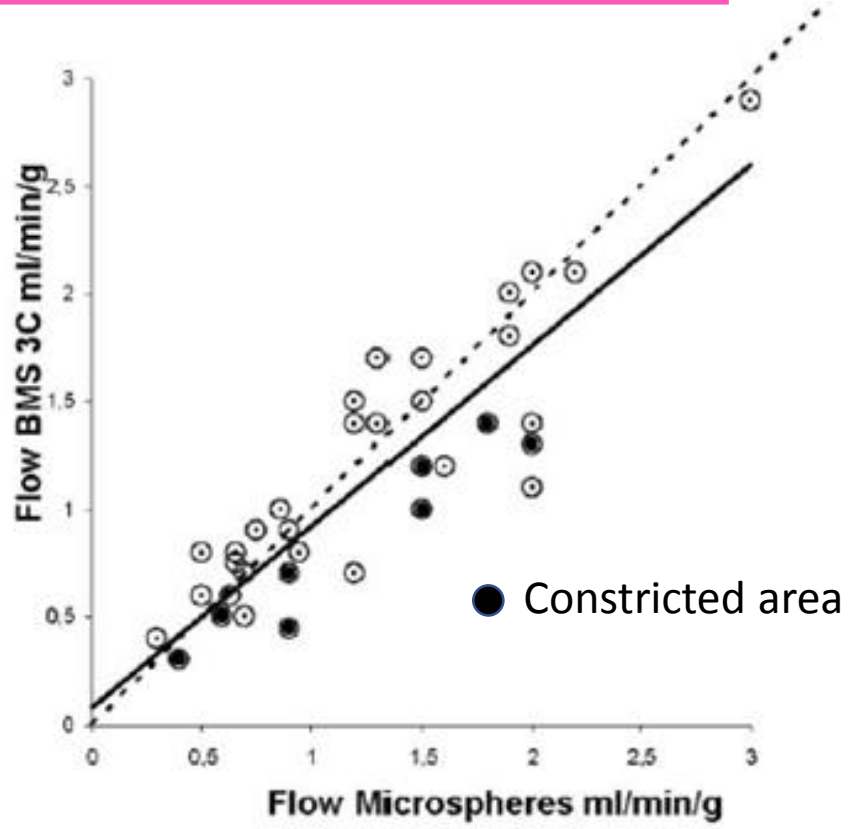
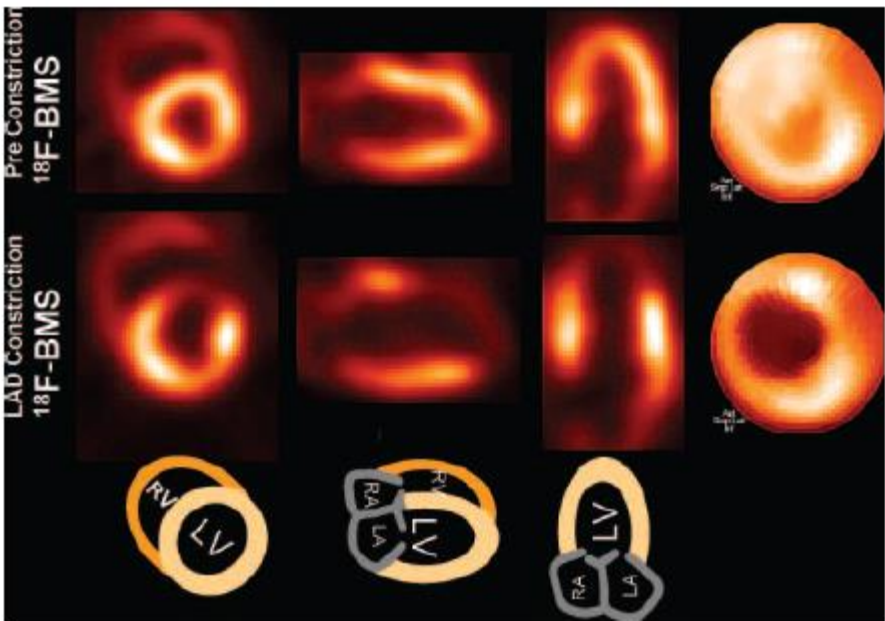
Kinetics of ^{18}F -BMS-747158-02 in myocardium



Nekolla et al., Circulation 2009, 119:2333-2342:

MBF comparison: ^{18}F -BMS-747158-02 vs microsphere

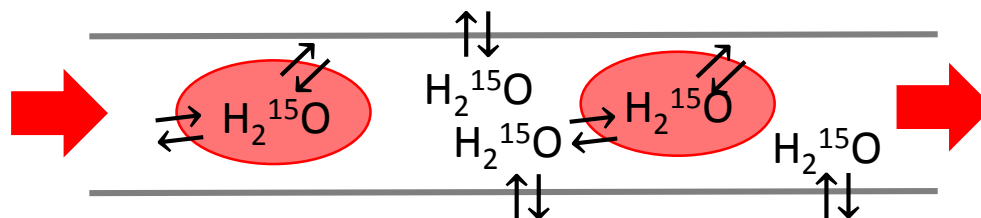
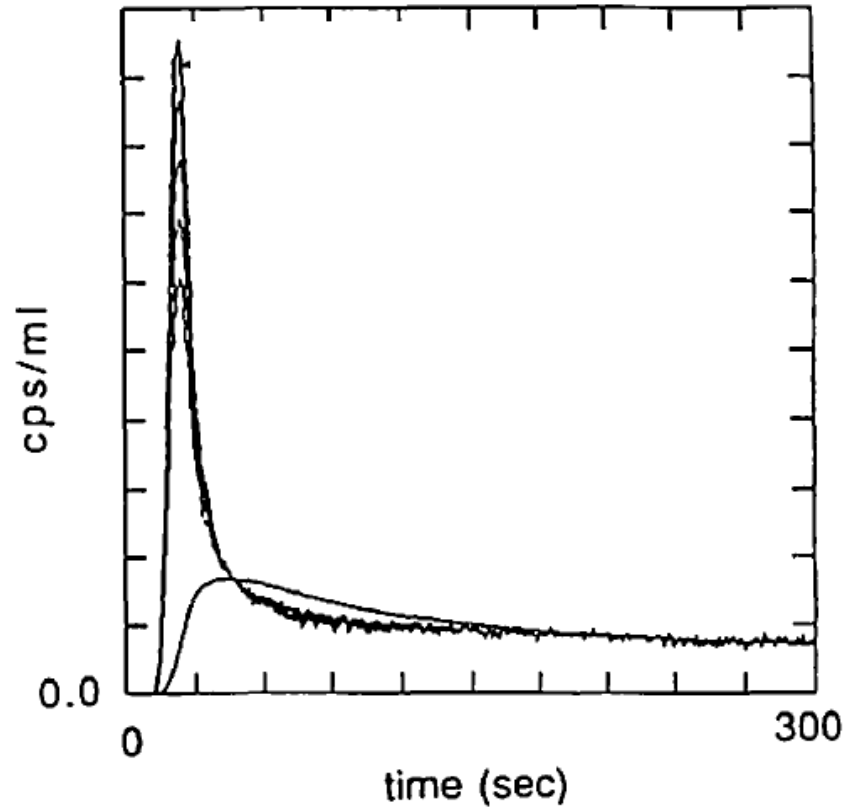
In normal and constricted LAD regions in pigs



Reduced MBF in constricted area than microsphere

Nekolla et al., Circulation 2009, 119:2333-2342:

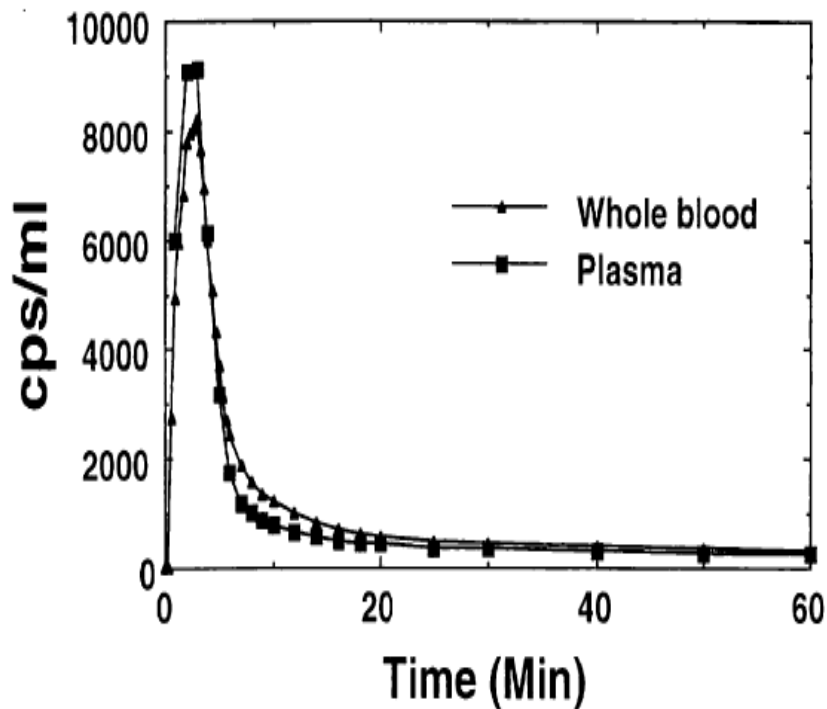
Whole blood radioactivity concentration as Input Function in $H_2^{15}O$



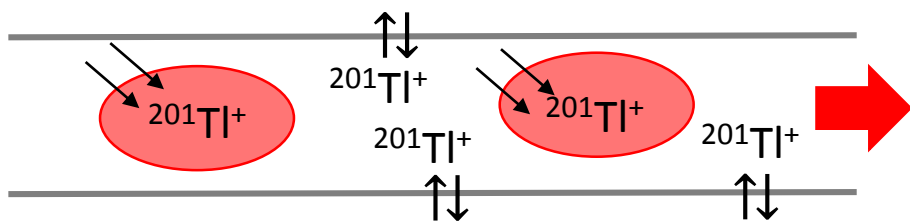
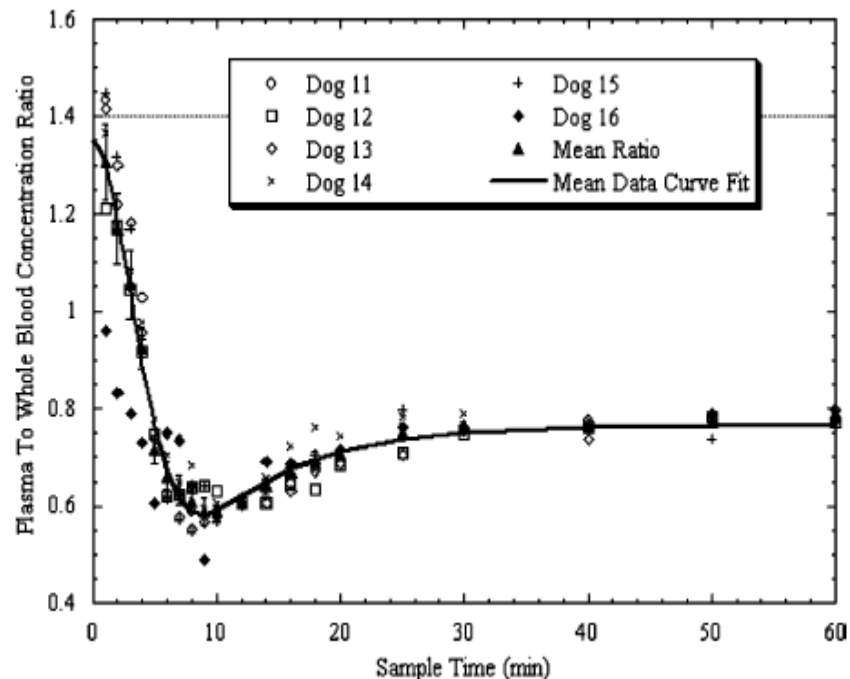
Plasma/whole blood ratio

^{201}Tl (also in ^{82}Rb ?)

Arterial input functions



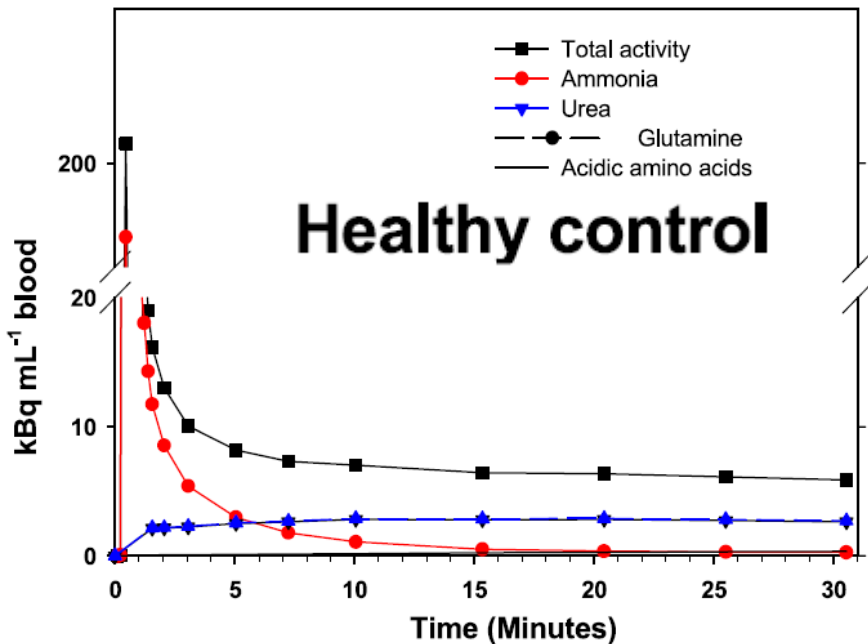
Plasma/whole blood ratio



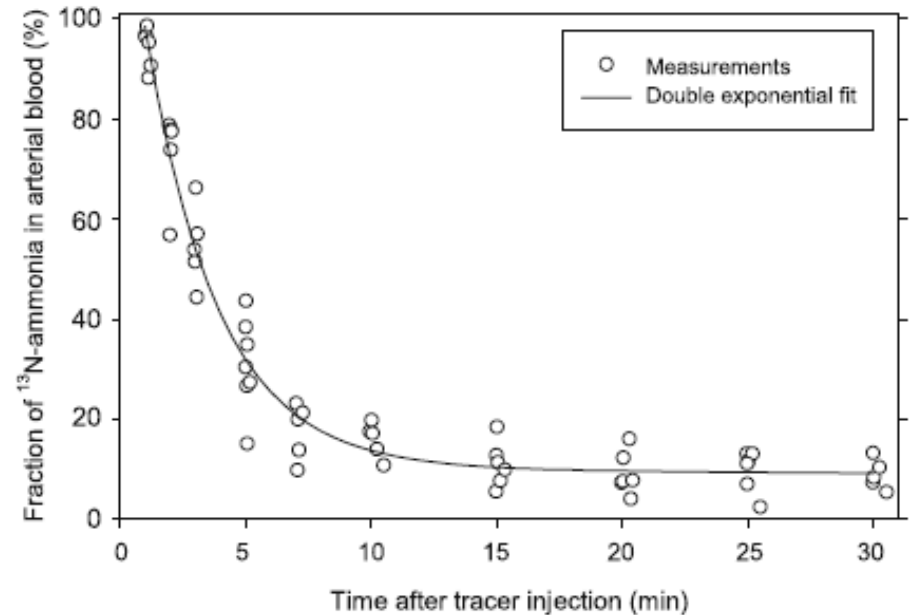
Iida et al., J Nucl Cardiol, 1998
Iida et al., J Nucl Med 2009

Metabolites in arterial blood in $^{13}\text{NH}_3$ PET

Arterial concentration (kBq/mL)



Fraction of $^{13}\text{NH}_3$ in blood (%)



Frequent diagnostic errors in cardiac PET/CT due to mis-registration of CTAC and emission PET images

CT-AC is often acquired during a breath hold, while PET assesses average over respirator & contractile motion

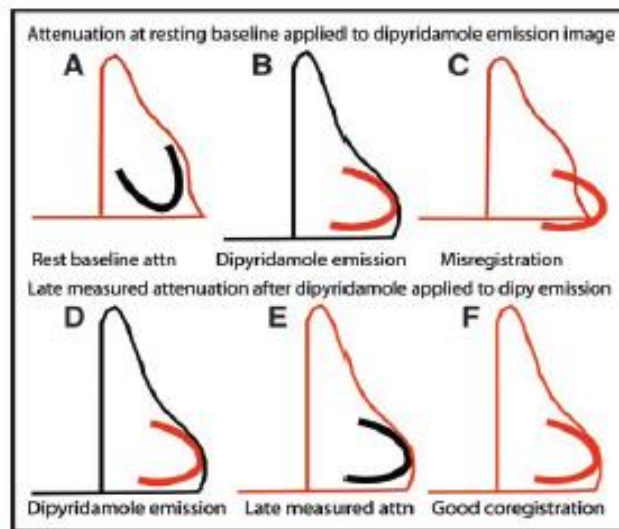
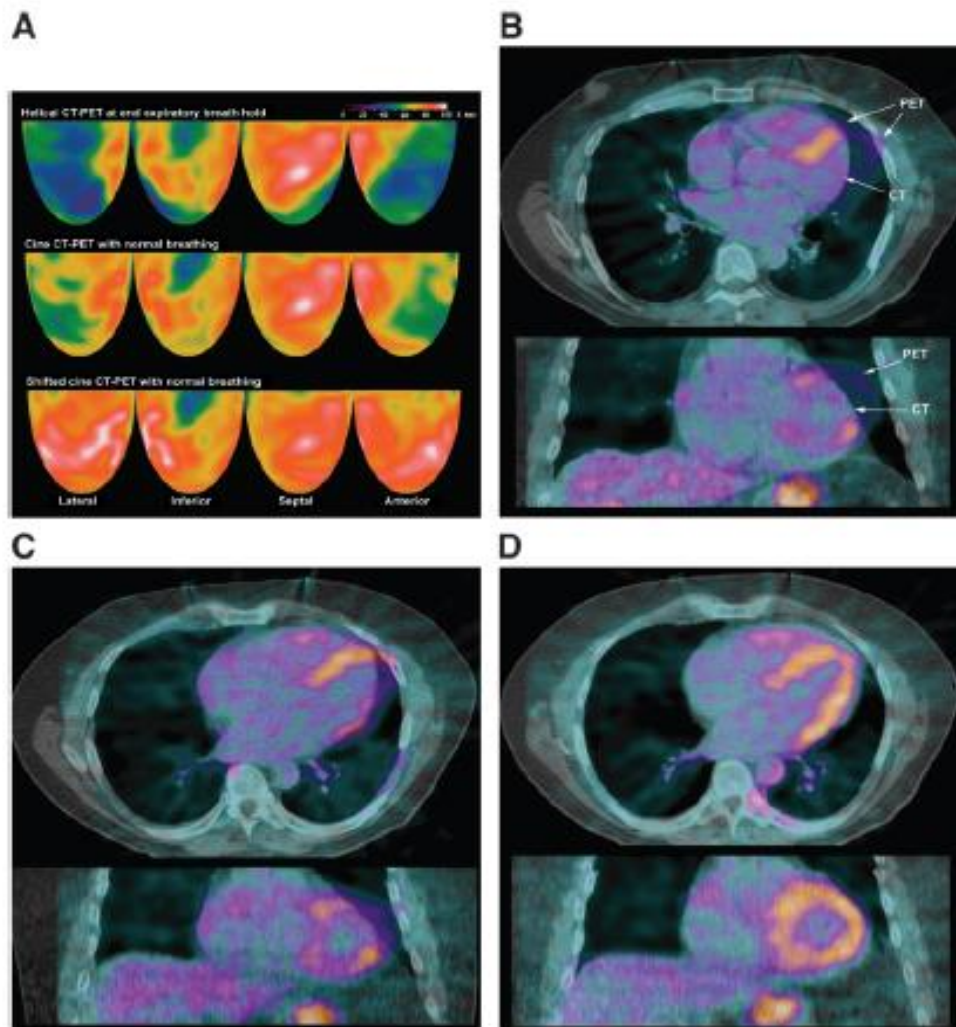


FIGURE 7. Mechanisms for attenuation artifacts using post-dipyridamole scan. Legend is the same as Figure 6.

Gould KL et al., JNM, 2007
Loghin C et al., JNM, 2004

Summary/comments

1. Regional myocardial blood flow as a flux of the tracer to/from tissue through the capillary membrane
2. Regional myocardial blood flow can be quantitatively assessed using PET and several radio-labeled tracers.
3. ^{15}O -water PET can provide accurate quantitative values and has been considered a gold standard
4. Step-by-step specification is encouraged not only for core software, but also for all intermediate processes including GUIs, by means of ISO13485 or equivalent processes
5. Mismatch between CT-AC and PET needs further technological innovation and development